

This Page Is Inserted by IFW Operations
and is not a part of the Official Record

BEST AVAILABLE IMAGES

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images may include (but are not limited to):

- BLACK BORDERS
- TEXT CUT OFF AT TOP, BOTTOM OR SIDES
- FADED TEXT
- ILLEGIBLE TEXT
- SKEWED/SLANTED IMAGES
- COLORED PHOTOS
- BLACK OR VERY BLACK AND WHITE DARK PHOTOS
- GRAY SCALE DOCUMENTS

IMAGES ARE BEST AVAILABLE COPY.

**As rescanning documents *will not* correct images,
please do not report the images to the
Image Problem Mailbox.**



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶: A61C 1/00, 3/00, 5/00	A1	(11) International Publication Number: WO 95/32679 (43) International Publication Date: 7 December 1995 (07.12.95)
(21) International Application Number: PCT/US95/05852 (22) International Filing Date: 11 May 1995 (11.05.95) (30) Priority Data: 08/251,135 31 May 1994 (31.05.94) US (71) Applicant: MEDICAL LASER TECHNOLOGY, INC. [US/US]; P.O. Box 6796, Hilton Head Island, SC 29938 (US). (72) Inventors: KOWALYK, Kenneth; 22 Compass Point, Hilton Head Island, SC 29928 (US). MYERS, Michael, J.; 5101 Newport, Hilton Head Island, SC 29928 (US). (74) Agents: GATTO, James, G. et al.; Baker & Botts, L.L.P., The Warner, 1299 Pennsylvania Avenue, N.W., Washington, DC 20004 (US).		(81) Designated States: AM, AT, AU, BB, BG, BR, BY, CA, CH, CN, CZ, DE, DK, EE, ES, FI, GB, GE, HU, IS, JP, KE, KG, KP, KR, KZ, LK, LR, LT, LU, LV, MD, MG, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, TJ, TM, TT, UA, UG, UZ, VN, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG), ARIPO patent (KE, MW, SD, SZ, UG). Published With international search report.
(54) Title: DENTAL LASER APPARATUS AND METHOD (57) Abstract <p>A method of ablating non-metallic dental material from a tooth comprises the steps of generating radiation pulses having a predetermined wavelength, energy level, pulse repetition rate, and duration, and applying the radiation pulses to the non-metallic dental material (15) in a tooth (18), whereby the non-metallic dental material is ablated from the tooth. The radiation may be generated by a frequency tripled Nd:YAG, an Er:YAG laser or an Er:YsGG laser and may have a wavelength of about 355 nanometers, 2.94 micrometers, and 2.79 micrometers respectively, for example.</p> <div data-bbox="860 1071 1315 1470" data-label="Image"> </div>		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	GB	United Kingdom	MR	Mauritania
AU	Australia	GE	Georgia	MW	Malawi
BB	Barbados	GN	Guinea	NE	Niger
BE	Belgium	GR	Greece	NL	Netherlands
BF	Burkina Faso	HU	Hungary	NO	Norway
BG	Bulgaria	IE	Ireland	NZ	New Zealand
BJ	Benin	IT	Italy	PL	Poland
BR	Brazil	JP	Japan	PT	Portugal
BY	Belarus	KE	Kenya	RO	Romania
CA	Canada	KG	Kyrgyzstan	RU	Russian Federation
CF	Central African Republic	KP	Democratic People's Republic of Korea	SD	Sudan
CG	Congo	KR	Republic of Korea	SE	Sweden
CH	Switzerland	KZ	Kazakhstan	SI	Slovenia
CI	Côte d'Ivoire	LI	Liechtenstein	SK	Slovakia
CM	Cameroon	LK	Sri Lanka	SN	Senegal
CN	China	LU	Luxembourg	TD	Chad
CS	Czechoslovakia	LV	Latvia	TG	Togo
CZ	Czech Republic	MC	Monaco	TJ	Tajikistan
DE	Germany	MD	Republic of Moldova	TT	Trinidad and Tobago
DK	Denmark	MG	Madagascar	UA	Ukraine
ES	Spain	ML	Mali	US	United States of America
FI	Finland	MN	Mongolia	UZ	Uzbekistan
FR	France			VN	Viet Nam
GA	Gabon				

DENTAL LASER APPARATUS AND METHOD

BACKGROUND OF THE INVENTION

Laser radiation techniques, generally, are known. Additionally, laser radiation equipment has been used in recent years in dentistry to replace
5 certain mechanical dental tools which require the use of anesthetics to reduce the patient's sensitivity to pain. For example, U.S. Patent No. 5,281,141 to Kowalyk discloses a method of removing tooth decay using a laser having an output wavelength which corresponds to the absorption band of a substance applied to the tooth decay.

10 Another example is disclosed in U.S. Patent No. 5,194,005 to Levy. Levy discloses a method of applying laser radiation to a ceramic material to promote the growth of a crystal structure in that material and create a strong bond between the hydroxyapatite and the surrounding tooth material. Levy also discloses in U.S. Patent No. 5,020,995 the use of a laser for
15 removal of tooth and gum tissue at a wavelength of 1.06 micron together with a water/air mixture to control the thermal cutting action. In U.S. Patent No. 5,151,029, Levy discloses use of a laser for removal or hardening of metal in a tooth. Various other patents address dental laser techniques.

Dentists have long used metal or dental amalgam materials to repair
20 and protect teeth. Most of these materials, however, contain mercury. Further, because of the color and/or luster of the metals and amalgams, use of these materials in a visible portion of the mouth is generally cosmetically displeasing to many patients. Due to the poor cosmetics and concerns of potential mercury release associated with these metal and dental amalgam
25 materials, there has been a recent movement in dentistry towards the use of non-metallic dental materials rather than metal or dental amalgam materials. For example, composite materials, which generally comprise microscopic particles of silica or quartz in a resin matrix, have been used more frequently in recent years. Also, the use of other non-metallic dental

materials such as porcelain or ceramic restorations have been used as full crowns, inlays, and onlays in recent years.

These non-metallic dental materials, however, sometimes require removal. Due to differences in the coefficient of thermal expansion
5 between the tooth and composite materials filled within a cavity in the tooth, for example, microscopic cracks may occur in the tooth. These cracks cause leakage in the tooth which may lead to pain and/or deterioration of the tooth. Also, non-metallic dental materials eventually wear during use due to the forces of mastication and have a tendency to
10 stain over prolonged use. Therefore, when any of the above situations occur (or for other reasons), it is desirable for the non-metallic dental material to be fully or partially removed and replaced.

SUMMARY OF THE INVENTION

Accordingly, a need has arisen for an effective method of removing
15 non-metallic dental material without requiring the use of anesthetics. Further, a need has arisen for a method of using laser radiation to ablate non-metallic dental material from a tooth without damaging the underlying tooth.

It is an object of the present invention to provide a method to safely
20 ablate non-metallic dental material from a tooth using laser radiation.

More specifically, it is an object of the present invention to provide a method to remove composite, ceramic or porcelain materials from a tooth using laser radiation.

It is a further object to the invention to provide a dental laser
25 method for removing materials from a tooth without excessive heating of the tooth, without the need for anesthetics and without pain or discomfort to the patient. It is also a goal of the invention to provide a method of ablation without the noise and vibration of the dental drill, handpiece or lung aspiration concerns of dental air-abrasives.

According to the above objects of the present invention, a method of ablating non-metallic dental material from a tooth comprises the steps of generating radiation pulses having a predetermined wavelength energy level, pulse repetition rate and duration, and applying the radiation pulses having predetermined characteristics to non-metallic dental material in a tooth, whereby the non-metallic dental material is ablated from the tooth. Preferably, a laser having a wavelength in the range of 100-600 nm or 2,000-4,000 nm is used because the composite resin or other non-metallic dental material has a relatively high absorption in those ranges. A frequency

10 tripled Nd:YAG or an Er:YAG laser, which generates radiation having a wavelength of about 355 nanometers and 2.94 micrometers, respectively, may be used, for example. Preferably, the laser radiation pulses have a predetermined pulse repetition rate, average power, pulse duration and peak energy level.

15 Other objects and advantages of the present invention will become apparent to one of ordinary skill in the art upon review of the detailed description of the preferred embodiment.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 depicts an apparatus for ablating non-metallic dental material

20 from a tooth.

Fig. 2 depicts an apparatus according to the present invention ablating non-metallic dental material from a tooth.

DETAIL DESCRIPTION OF A PREFERRED EMBODIMENT

With reference to Figs. 1 and 2, a laser source 1 which is capable of

25 producing a laser beam 1a, an output coupler 2 and a mirror 3 which reflects the beam to a fiber coupler 4 are disclosed. Optionally, the laser beam 1a may be joined by an aiming beam 1b, which may be produced by diode 5, and which may travel coaxially with the laser beam, in a known manner, along a fiber optic cable 13 to a commercially available laser

handpiece 14. However, other delivery options and optical arrangements will be readily apparent and the invention is not limited to the described structure.

According to one method of the present invention, the laser beam
5 generated has characteristics sufficient to ablate non-metallic dental material in a tooth but not damage the tooth tissue or other matter surrounding the material. Non-metallic dental materials may comprise composite material, ceramic, porcelain, and synthetic hydroxyapatite, for example. Composite materials typically comprise microscopic particles of
10 silica or quartz in a resin matrix. When ablating composite materials, it may be desirable to only attack the resin matrix portion and thereby effectively ablate the composite material. The application of laser radiation using a fiber optic cable 13 applied using a commercially available laser handpiece 14, as depicted in Fig. 2, allows for the ablation of the non-
15 metallic dental material.

Due to their chemical composition, commercially available dental restorative materials exhibit higher optical densities in the 100-600 nm and 2,000-4,000nm wavelength range than natural tooth structure. Therefore, ablation using lasers generating radiation in these wavelength ranges may
20 be performed without damaging surrounding natural tooth structure. Lasers generating radiation having a wavelength in this range are potentially more efficient in the ablation of these materials than traditional dental tools, at lower powers and less energy.

Laser source 1 may be, for example, an Nd:YAG laser (Neodymium,
25 yttrium aluminum garnet). To ablate the non-metallic dental material, the frequency of the laser may be tripled or shifted via OPO or Raman techniques to generate wavelengths corresponding to the desired spectral range, for example. Other methods of laser wavelength modification may also be used to provide a desired laser radiation wavelength. The

frequency tripled Nd:YAG laser may generate radiation pulses having a wavelength of about 355 nanometers, for example. The frequency tripled Nd:YAG laser may have a pulse repetition rate of between one and 10,000 pulses/sec, an average power of up to 100 watts, a pulse duration of between a pico second and several milliseconds, and a peak energy of up to five joules/pulse. For example, the frequency tripled Nd:YAG laser may be operated at a peak energy of about 20 milli-Joules having a pulse duration of about 30 nano-seconds, a frequency of about 20 Hz and provide an average power of about 400 milli-Watts. The frequency tripled Nd:YAG laser may also be Q-switched. These characteristics are determined by the ablation efficiency of the non-metallic dental materials. Low average powers with higher peak powers are preferred, so as not to cause pulpal damage in the tooth.

Another example of a suitable laser is the Er:YAG laser (erbium doped, yttrium aluminum garnet). This laser may generate radiation pulses having a wavelength of about 2.94 micrometers, for example. Another laser source that may be used is an Er:YSGG (erbium doped, yttrium scandium gallium garnet) laser generating radiation pulses having a wavelength of about 2.79 micrometers. The range for the pulse repetition rate, average power, pulse duration and energy of the Er:YAG and the Er:YSGG laser may also be similar to the frequency tripled Nd:YAG laser. For example, the Er:YSGG laser may be operated with a peak energy of about 250 milli-Joules, having a pulse duration of about 30 nano-seconds, a frequency of about 20 Hz and providing an average power of 400 milli-Watts.

Other lasers may also be used having similar ranges of operation. Lasers such as the Argon laser (514), doubled Nd:GSGG (1061-530nm), Nd:YV04 (1064-532nm), Nd:KGW (1060-530nm), Nd:Phosphate glass (1053-526nm), Nd:YAP (1080-540nm), Nd:GGG/GSGG (1064-532nm), Nd:YLP (1053-526nm + 1047-523nm), Nd:YALO/YAP (1080-540nm),

Cr:Fosterite (1235-617nm), Alexandrite (755-377nm), Nd:GdVO₄ (1060-530nm), Ti:Sapphire (800-400nm), Cr:LiSAF/LiCAF (840-420nm), and Nd:Silicate glass (1062-531nm), for example, may be used. Some of these other laser materials are tunable within various output wavelength regions
5 near those values indicated above.

The method of ablating non-metallic dental material generally comprises using laser source 1 to generate laser radiation pulses. These laser radiation pulses are applied through output coupler 2, fiber coupler 4, and a fiber optic cable 13 to a commercially available laser handpiece 14.
10 This handpiece may comprise a tip 16 comprising an optical fiber which is connected to fiber optic cable 13 and therefore receives and transmits the laser radiation pulses generated by laser source 1. Tip 16 then may be applied to the composite material 15 in a tooth 18. The laser radiation thus ablates composite material 15, but due to the selected wavelength leaves
15 unharmed the tooth tissue of tooth 18 underlying composite material 15 because of the wavelength of the radiation applied thereto. Composite material 15 may also be ceramic, porcelain, or any other type of non-metallic dental material, for example.

Flushing of ablated material using air and/or water or other fluids
20 and gases such as fluorocarbons and nitrogen, for example, may be used to remove the ablated material from the area where the radiation pulses are being applied. This increases efficiency by avoiding the situation where lasing of the ablated particles occurs. Depending on the laser used and its frequency (and other characteristics) one type of fluid may be preferred
25 over another. For example a fine spray of water and air may be used to flush away the ablated material when using the Er:YSGG and Er:YAG lasers. A simultaneous jet of air may be used to remove ablated material when using the frequency tripled Nd:YAG laser, however, the invention is not so limited. The type and amount of fluid and/or gas used is

determined based on the inherent photophysical properties encountered with the laser/material interaction.

The foregoing is a description of an embodiment of the present invention. The invention is not limited to the foregoing description, but
5 rather, is to be limited only by the claims appended hereto. Numerous variations and modification will be apparent to one of ordinary skill in the art within the scope of the invention.

CLAIMS

What is claimed is:

1. A method of ablating a non-metallic dental material from a tooth comprising the steps of:
 - 5 generating radiation pulses having a predetermined wavelength, energy level, pulse repetition rate and duration; and
 - applying the radiation pulses to the non-metallic dental material in a tooth;
- whereby the non-metallic dental material is ablated from the tooth.
- 10 2. The method of claim 1, wherein the non-metallic dental material comprises a composite material having a resin component and whereby the radiation pulses ablate the resin component.
3. The method of claim 1, wherein the radiation pulses are generated by a frequency tripled Nd:YAG laser having a wavelength of about 355
- 15 nanometers.
4. The method of claim 3, wherein the radiation pulses are generated by a Er:YSGG laser generation radiation pulses having a wavelength of about 2.79 micrometers.
5. The method of claim 1, wherein the radiation pulses are generated
- 20 by an Er:YAG laser generating radiation pulses having a wavelength of about 2.94 micrometers.
6. The method of claim 1, wherein the non-metallic dental material comprises ceramic.
7. The method of claim 1, wherein the non-metallic dental material
- 25 comprises porcelain.
8. The method of claim 1 further comprising the step of flushing ablated non-metallic material.

9. A method of ablating a non-metallic dental material from a tooth comprising the steps of:
- providing an optical fiber having an input end and an output end;
 - applying the output end of said optical fiber to the non-metallic
 - 5 dental material in a tooth; and
 - generating radiation pulses on the input end of the optical fiber;
 - whereby the radiation pulses are applied to the non-metallic dental material through the optical fiber and ablate the non-metallic dental material in the tooth.
- 10 10. The method of claim 9, wherein the non-metallic dental material comprises a composite material having a resin component and whereby the radiation pulses ablate the resin component.
11. The method of claim 9, wherein the radiation pulses are generated by a frequency tripled Nd:YAG laser.
- 15 12. The method of claim 9, wherein the radiation pulses are generated by an Er:YAG laser.
13. The method of claim 9, wherein the radiation pulses are generated by an Er:YSGG laser.
14. An apparatus for ablating non-metallic dental material from a tooth
- 20 comprising:
- means for generating radiation pulses; and
 - means for applying the radiation pulses to non-metallic dental material in a tooth; whereby said non-metallic dental material is ablated from the tooth.
- 25 15. The apparatus of claim 14, wherein the non-metallic dental material comprises a resin component and whereby the radiation pulses ablate the resin component of the non-metallic dental material.
16. The apparatus of claim 14, wherein the means for generating radiation pulses comprises a frequency tripled Nd:YAG laser.

17. The apparatus of claim 14, wherein the means for generating radiation pulses comprises an Er:YAG laser.
18. The apparatus of claim 14, wherein the means for generating radiation pulses comprises an Er:YSGG laser.
- 5 19. The apparatus of claim 14, wherein the non-metallic dental material comprises ceramic.
20. The apparatus of claim 14, wherein the non-metallic dental material comprises porcelain.
21. The apparatus of claim 14 further comprising means for flushing
10 ablated non-metallic material.

1/1

FIG. 1

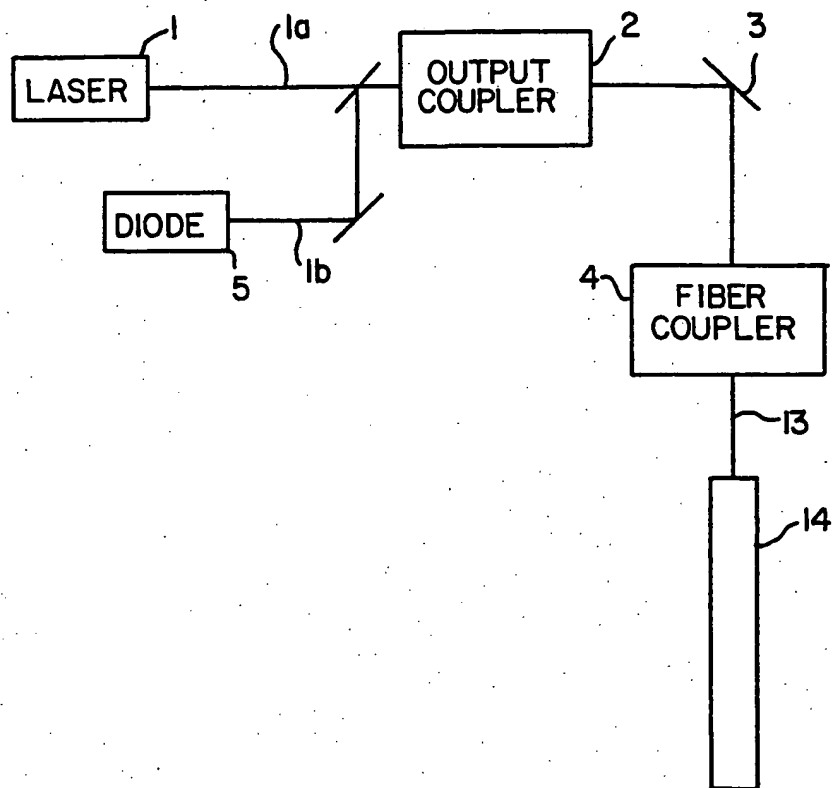
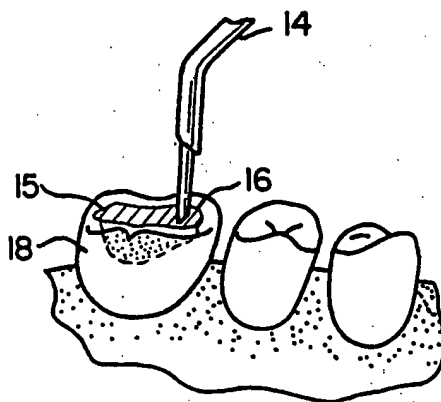


FIG. 2



SUBSTITUTE SHEET (RULE 26)

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US95/05852

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) :A61C 1/00; 3/00; 5/00
US CL :433/29, 215

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 433/29, 215

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

APS "dental and laser and remov? and filling and ablate and amalgam"

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X --- Y	US, A, 5,267,856 (WOLBARSHT ET AL) 07 December 1993, see col. 3, lines 49-65.	1,5-9,12,14 17,19-21
A	US, A, 5,092,772 (LEVY) 03 March 1992, see the entire document.	2-4,10,11, 13,15,16, 18
A	US, A, 5,180,304 (VASSILIADIS) 19 January 1993, see the entire document.	13, 15, 16, 18
A	US, A, 5,194,005 (LEVY) 16 March 1993, see the entire document	1-18
		1-18

☒ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	T	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
*A		document defining the general state of the art which is not considered to be part of particular relevance
*E	X	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
*L	Y	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
*O		document referring to an oral disclosure, use, exhibition or other means
*P	A	document published prior to the international filing date but later than the priority date claimed

Date of the actual completion of the international search

09 AUGUST 1995

Date of mailing of the international search report

22 AUG 1995

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
Box PCT
Washington, D.C. 20231

Facsimile No. (703) 305-3230

Authorized officer

NICK LUCCHESI

Telephone No. (703) 308-2698

INTERNATIONAL SEARCH REPORTInternational application No.
PCT/US95/05852

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A, P	US, A, 5,409,376 (MURPHY) 25 April 1995, see the entire document.	1-18